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1 **The fabrication of a flexible and portable sensor based on home-made laser-**  
2 **induced porous graphene electrode for the rapid detection of sulfonamides**

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13 **Abstract**

14 A smartphone-based wireless electrochemical sensor for portable and fast  
15 detection of sulfonamides (SAs) using home-made flexible integrated three-electrode  
16 of laser-induced porous graphene (LIPG) modified with two-dimensional hexagonal  
17 boron nitride (2D h-BN) as working electrode was developed. The flexible integrated  
18 three-electrode of LIPG was prepared by direct laser-writing technique on polyimide  
19 (PI) film. The reference electrode was handmade by casting a silver and silver  
20 chloride ink on the surface of the LIPG. With excellent electrochemical performance,  
21 the pocket, disposable, cost-effective, flexible three-electrode constructed a novel  
22 sensing platform to detect sulfamethoxazole (SMZ) at a lower electrochemical  
23 oxidation potential of 0.56 V. The developed sensor displayed a good linear range  
24 from 0.5 to 362.5  $\mu\text{M}$ , a low limit of detection was 0.011  $\mu\text{M}$  and satisfactory  
25 recovery in the range of 97.5% - 101.3% in milk and lake water. This sensor was also  
26 applied for the detection of four other SAs (sulfanilamide, sulfapyridine,  
27 sulfadimidine, sulfisoxazole). This work will be valuable to the development of a  
28 simple, fast sensing platforms for outdoor detection and online monitoring in food  
29 safety and environmental safety areas.

30 **Keywords:** Flexible sensor; Integrated three-electrode; Sulfonamides; Laser-induced  
31 porous graphene; Hexagonal boron nitride

## 32 1. Introduction

33 Sulfonamides (SAs), a broad-spectrum antibacterial drug with *p*-aminobenzene  
34 sulfonamide, are widely used around the world due to their stable chemical properties,  
35 convenient use and low price. But a large amount of production and excessive or  
36 irrational application of antibiotics has induced various risk in food contamination and  
37 environmental pollution. Sulfamethoxazole (SMZ), one of the representatives of  
38 sulfonamides antibiotics, plays an important role in preventing and treating infections.  
39 As a highly persistent pollution, SMZ has large toxicological effects in animal-  
40 derived food and aquatic environment [1,2], and it is one of three sulfonamides (the  
41 other two are sulfisoxazole and sulfamethazine) have been classified as a Category 3  
42 carcinogen by the World Health Organization. When exposing to a low level of  
43 antibiotics over a long period of time, humans may suffer from the risk of antibiotic  
44 resistance and even thyroid cancer [3,4]. In China, European Union and other  
45 countries, the safe limit for sulfonamide residues should not exceed  $100 \mu\text{g}\cdot\text{kg}^{-1}$  in  
46 edible animal tissue and should not exceed  $25 \mu\text{g}\cdot\text{kg}^{-1}$  in milk. Therefore, the  
47 development of effective and convenient methods to detect residual antibiotics from  
48 food and water is imperative [5].

49 SMZ and other SAs have normally been detected by laboratory-based analytical  
50 techniques, such as chromatography and coupled to other methods, fluorescence  
51 techniques [6-8], which can provide good qualitative or quantitative information.  
52 However, these techniques require expensive and bulky equipment, a lot of time in  
53 complicated sample preparation and are limited to use in the laboratory. It cannot

54 meet the requirements of the trending of simple, quick, portable, and low-cost tests for  
55 antibiotic residues analysis. Electrochemical sensors are the most promising method  
56 due to its low cost, simple operation, and fast response in trace analysis [9-13]. In  
57 recent years, electrochemical sensors are developing towards miniaturization,  
58 integration, networking and intelligence, which has been used for trace analysis of  
59 hazardous substances [14-18].

60 With the development of portable devices, the smart and miniaturized sensors for  
61 on-site fast detecting have become one of the hotspots in the field of sensing.  
62 However, the conventional rigid electrodes cannot meet this requirement, hence the  
63 research of flexible and pocket electrode has attracted extensive attention in the  
64 worldwide. A flexible electrode based on laser-induced porous graphene (LIPG) using  
65 laser direct writing technology has been studied in our laboratory for several years,  
66 and it had successfully deployed in electrochemical sensors for practical usage in  
67 evaluation of fish freshness, intelligent analysis of phytohormone and SAs [19-23].  
68 But so far, the research on LIPG is only limited to the preparation and application of  
69 the flexible working electrode, while this study focused on the flexible integrated  
70 three-electrode (working electrode, reference electrode and counter electrode) based  
71 on LIPG is few reported. Although commercial screen-printed electrodes (SPCE) as  
72 three-electrode system combined with portable sensors and smartphone are currently  
73 available for convenient detection of antibiotics including SAs [24,25], the high limit  
74 of detection (LOD) and high electrochemical oxidation potential for sulfamethoxazole  
75 is not ideal [26,27]. The three-electrode system is still in its infancy, its tremendous

76 application foreground in portable sensing analysis and outdoor detection has great  
77 research value. In our study, a flexible integrated three-electrode was prepared on  
78 polyimide (PI) film using direct laser-writing technique, the working electrode (can be  
79 chemically modified) and the auxiliary electrode is bare LIPG, the reference electrode  
80 was handmade by casting silver and silver chloride ink on the porous graphene  
81 conducting track. The homemade flexible integrated three-electrode can fit perfectly  
82 with a portable mini-workstation and can be connected to a smartphone via Bluetooth.  
83 It not only replaced glassy carbon electrode coupled with both traditional large-scale  
84 workstation and tablet computer, but has a lower catalytic potential than SPCE.  
85 Meanwhile, the surface modification of the working electrode of flexible integrated  
86 three-electrode is very important to enhance the electrochemical sensing performance  
87 for SMZ.

88 Two-dimensional (2D) materials have attracted extensive research interest due to  
89 their unique physicochemical properties. Hexagonal boron nitride (h-BN) as an  
90 emerging 2D material, consisting of boron and nitrogen atoms aligned in a hexagonal  
91 structure via the strong covalent bonds and weak Van der Waals bilayer interaction.  
92 Overturning the initial reports that h-BN was non-conductive, researchers began  
93 applying 2D h-BN to the field of electrochemistry, particularly in electrochemical  
94 sensing fields [28,29]. It plays a prominent role in promoting the development of  
95 electrochemical sensors due to its large surface area, remarkable electron transport  
96 capabilities, and rich chemical stability [30,31].

97 Inspired by these aspects, we demonstrated a novel wireless electrochemical

98 sensor based on the home-made flexible integrated three-electrode for portable and  
99 fast detection of SAs, including SMZ, sulfanilamide (SN), sulfisoxazole (SIZ),  
100 sulfamethazine (SM2) and sulfapyridine (SPY). SMZ as one of the SAs carcinogens  
101 was used as the model analyte to optimize experimental conditions, and study the  
102 surface morphology and performance (electrochemical oxidation potential,  
103 electrochemical behaviors, cycle stability, electrochemically effective surface areas,  
104 repeatability, reproducibility and selectivity) of the home-made flexible integrated  
105 three-electrode. The flexible integrated three-electrode coupled with a portable mini  
106 electrochemical workstation was successfully applied for the determination of SMZ in  
107 milk and lake water. Finally, it was proved suitable for the detection of four SAs  
108 including SN, SIZ, SM2, SPY.

## 109 **2. Experimental section**

### 110 2.1. Materials

111 SMZ, SN, SIZ, SM2, and SPY (power form, purity  $\geq 99\%$ ) was purchased from  
112 Stanford Analytical Chemicals Inc., and its stock solution was prepared with  
113 methanol. Silver and silver chloride ink (Ag/AgCl ink, YTXD-50-20, fineness  $\leq 20$   
114  $\mu\text{m}$ ) and special thinner was obtained from Suzhou Yituo Biosensor Technology Co.,  
115 Ltd. Pristine h-BN nanoflake solution (purity  $> 99\%$ , sheet diameter from 50 to 200  
116 nm) was obtained from Nanomaterial Technology Co., Ltd (Jiangsu, China).  
117 Commercial-available polyimide (PI) film (Kapton tape, thickness: 80  $\mu\text{m}$ ), a polymer  
118 sheet was used to fabricate the flexible integrated three-electrode composing of LIPG,  
119 was purchased from DuPont Company, America. 0.04  $\text{mol}\cdot\text{L}^{-1}$  (0.04 M) Britton-

120 Robinson (BR) buffer solution was used as supporting electrolyte and prepared with  
121 mixing stock solution of phosphoric acid, acetic acid, and boric acid. The various pH  
122 of the BR buffer was regulated by 0.01 M NaOH. All other reagents were analytical  
123 grade and no further purification unless otherwise stated. Deionized water (DI water,  
124  $18.2 \text{ M}\Omega \cdot \text{cm}$ ) was obtained from a Milli-Q water purification system and used in all  
125 experiments.

## 126 2.2. Instruments

127 The laser-induced process was carried out under ambient conditions using a  
128 home-made computer-controlled laser-scribing micromachining system (Nano Pro-  
129 III, Tianjin Jiayin Nanotechnology Co., Ltd., China, wavelength = 450 nm, precision  
130 =  $10 \mu\text{m}$ , maximum power = 5.2 W, output laser beam  $< 10 \mu\text{m}$ , carving speed =  $0.5$   
131  $\text{cm s}^{-1}$ ). A LIPG integrated three-electrode system consisting a partially unmodified  
132 LIPG served as a counter electrode, Ag/AgCl ink was casted on the porous graphene  
133 conductive track as the reference electrode, the three-electrode where the working  
134 electrode part was not modified was named LIPG<sub>0</sub>, and it was named h-BN/LIPG<sub>0</sub>  
135 after being modified with h-BN. Portable mini electrochemical workstation with the  
136 PS Trace program was obtained from Red Matrix China Limited (PalmSens,  
137 Netherlands). The size of the portable mini electrochemical workstation is  $10.0 \times 6.0$   
138  $\times 3.4 \text{ cm}$ , weight is 250 g, battery is PS3BATT. A traditional electrochemical  
139 workstation was obtained from Shanghai Chenhua Instrument Co., Ltd (CHI 620E,  
140 China). Chromatographic analysis was implemented by high performance liquid  
141 chromatography (HPLC) analyzer (Waters E2695, USA). SPSS (22.0) Statistical



142 Analysis Software was used to compare the obtained results using the proposed  
143 electrochemical sensing method and HPLC.

### 144 2.3. Synthesis of LIPG electrodes

145 Before the preparation process, a home-made computer-controlled laser scribing  
146 machine (wavelength = 450 nm, precision = 10  $\mu\text{m}$ , maximum power = 5.2 W, output  
147 laser beam < 10  $\mu\text{m}$ , carving speed = 0.5  $\text{cm s}^{-1}$ ) was preheated for 30 min. To reduce  
148 cost and incorporation functionality, PI film was applied as a flexible, reliable  
149 platform for a PI film substrate was tailored into proper size, and cleaned by DI water,  
150 ethanol and DI water for several times, and was fixed on a glass plate to avoid shape  
151 deformation [19]. Then, a batch of original LIPGs was prepared under ambient  
152 conditions according to a designed drawing (Fig. S2A), and individual electrodes  
153 were carefully cut off with scissors. Finally, reference electrode was modified with  
154 Ag/AgCl ink to obtain a complete and LIPG<sub>0</sub>. A piece of PI film was pasted on the  
155 long conducting part to isolate the working area and only the working area was in  
156 contact with the electrolyte solution.

157 LIPG<sub>0</sub> without reference electrode part was obtained according to the above  
158 steps, which was labeled as LIPG<sub>1</sub>. LIPG<sub>1</sub> and saturated calomel electrode (SCE, as  
159 the reference electrode) was used to form a three-electrode system. Working  
160 electrode was modified with h-BN, and dried under infrared light to obtain h-  
161 BN/LIPG<sub>0</sub> flexible integrated three-electrode.

### 162 2.4. Electrochemical measurements

163 The quantification of SMZ was operated in 5 mL 0.04  $\text{mol}\cdot\text{L}^{-1}$  (0.04 M) BR

164 buffer (pH = 5.0) by h-BN/LIPG<sub>0</sub> flexible integrated three-electrode, which was  
165 perfectly plugged into the portable mini electrochemical workstation interface and  
166 connect wirelessly to a smartphone via Bluetooth. The voltammetric analysis of SMZ  
167 and the optimization of experimental parameters were by differential pulse  
168 voltammetry (DPV) with the potential range of 0.2 - 1.2 V, the step potential of 0.004  
169 V, the pulse potential of 0.05 V, the pulse width of 0.02 s. In 5 mM K<sub>3</sub>[Fe(CN)<sub>6</sub>] and  
170 K<sub>4</sub>[Fe(CN)<sub>6</sub>] containing 0.1 M KCl solution, the electrochemical behaviors and  
171 electro-oxidation mechanism with changeable scanning rate were performed by cyclic  
172 voltammetry (CV) with the step potential of 0.01 V. To contrast their performance  
173 potential, LIPG flexible integrated three-electrode was tested using a portable mini  
174 electrochemical workstation with a smartphone in comparison with traditional an  
175 electrochemical workstation with a desktop computer combined with both SCE and  
176 LIPG<sub>1</sub>.

### 177 2.5. Real sample preparation

178 Lake water (collected from Jiangxi Agricultural University) was filtered using a  
179 0.22 μm filter to remove the suspended particles. The filtered water sample was  
180 diluted with BR buffer (pH = 5.0). Commercial milk was acquired in a local market  
181 and was treated according to the following procedure: 40 mL of BR buffer/ACN 50%  
182 (v/v) was added to 5 g of milk and sonicated for 30 min. The mixture was then  
183 centrifuged at 4000 rpm for 15 min and filtered through a 0.22 μm filter. The filtrate  
184 was diluted with BR (pH = 5.0) to 50 mL to obtain the samples. To verify SMZ in real  
185 samples, recoveries of spiked samples were detected using the proposed method and

186 HPLC method.

## 187 2.6. Method validation

188 The assessment of validation parameters included linearity, LOD, and limit of  
189 quantification (LOQ), recovery and precision. The linearity was verified using buffer  
190 solution at ten concentration levels within the range of 0.50 – 362.5  $\mu\text{M}$  for  
191 electrochemical sensor and the range of 0 - 39.5  $\mu\text{M}$  for HPLC. We determined LOD  
192 and LOQ by repeating the blank test that can calculate the standard deviation ( $S_d$ ) of  
193 blank test with signal to noise ratios (S/N) of 0.011  $\mu\text{M}$  for LOD and 0.037  $\mu\text{M}$  for  
194 LOQ. Recovery was determined by spiking two kinds of blank samples with the  
195 standard solution of SMZ at two levels: 27.5  $\mu\text{M}$  and 55.0  $\mu\text{M}$ . Precisions of the two  
196 methods were assessed by repeatability experiments in three replicates and expressed  
197 as the relative standard deviations (RSD).

## 198 3. Results and discussion

### 199 3.1 Preparation of flexible integrated electrode

200 One-step laser scribing on commercial PI films in air to form 3D porous  
201 graphene layers and then Ag/AgCl ink was drop-coated to a specific part to obtained  
202 individual LIPG<sub>0</sub> electrodes ([Scheme 1](#)). Firstly, a series of electrodes on PI sheet  
203 were fabricated by the laser scribing technique, and then the individual electrode was  
204 obtained by carefully cutting off with scissors. Secondly, the electrode area in contact  
205 with the solution is selectively passivated by a piece of PI film, where the diameter of  
206 working electrode was 3 mm. Finally, the flexible and integrated three-electrode  
207 (LIPG<sub>0</sub>) was obtained. A comparison of LIPG<sub>0</sub> electrode with a paper clip was shown

208 in Fig. S2B, indicating the prepared LIPG<sub>0</sub> electrode was very pocket and portable.

209 The LIPG<sub>0</sub> electrode (drop-coated Ag/AgCl ink as reference electrode) was  
210 electrochemically modified in a specific part with h-BN to obtain the flexible  
211 integrated h-BN/LIPG<sub>0</sub> electrode. The flexible integrated electrode of h-BN/LIPG<sub>0</sub>  
212 was fit into a mini portable workstation and connects to the smartphone through  
213 Bluetooth to build a wireless sensor. The inset SEM image and voltammetry of 50  
214 cycles presented the 3D porous surface and the stability of the LIPG<sub>0</sub> electrode. The  
215 electrochemical catalytic mechanism and rapid analysis of SMZ on the h-BN/LIPG<sub>0</sub>  
216 electrode were shown in Scheme 1. Finally, the on-site detection of raw lake water  
217 with the flexible portable sensor was performed.

218 The surface morphologies of the prepared LIPG<sub>0</sub> electrode and h-BN/LIPG<sub>0</sub>  
219 electrode were characterized by SEM (scanning electron microscope), TEM  
220 (transmission electron microscope) and HAADF-STEM (high-angle annular dark-  
221 field-scanning transmission electron microscopy). The top-view SEM images of  
222 LIPG<sub>0</sub> electrode (Fig. 1A&B) and h-BN/LIPG<sub>0</sub> electrode (Fig. 1G&H) showed  
223 characteristic graphene fringes and an ordered-porous flake foam-like structure. As  
224 this laser scribing was performed in air, the local availability of oxygen and moisture  
225 could burn-off some of the carbon during the graphitization to release CO and CO<sub>2</sub>  
226 gases, resulting in the porosity [32]. The cross-sectional SEM images revealed that  
227 both LIPG<sub>0</sub> electrode (Fig. 1C&D) and h-BN/LIPG<sub>0</sub> electrode (Fig. 1I&J) had more  
228 porous structure in different sizes, but it seemed that the h-BN/LIPG<sub>0</sub> electrode had a  
229 more regular perforated structure and thicker section than LIPG<sub>0</sub> electrode. These

230 porous and thicker sections enabled h-BN/LIPG<sub>0</sub> electrode to have a large active area  
231 and facilitate electrolyte penetration into three-dimensional active materials.

232 The microstructures of both LIPG<sub>0</sub> and h-BN/LIPG<sub>0</sub> electrode were investigated  
233 by TEM. It can be seen that the LIPG<sub>0</sub> (Fig. 1E&F) and the h-BN/LIPG<sub>0</sub> (Fig. 1K&L)  
234 had ripple-like wrinkled structure with few-layer features, in which the h-BN/LIPG<sub>0</sub>  
235 was more uniform and distinct than the LIPG<sub>0</sub> electrode. According to the report of  
236 Lin [33], the ripples were exposed edges of graphene layers in high-resolution TEM  
237 image, and the formation of these ripples could be attributed to thermal expansion  
238 caused by laser irradiation. To further determine the dispersion of elements, HAADF-  
239 STEM and the corresponding energy dispersive X-ray (EDX) elemental mapping of  
240 C, O, B and N elements of the h-BN/LIPG<sub>0</sub> electrode were carried out. The  
241 corresponding result was presented in Fig. 1M-P, showing that the uniform  
242 distribution of C, O, B and N elements in the h-BN/porous graphene. SEM-EDS  
243 (scanning electron microscope/energy dispersive X-ray spectrometer) image (Fig. 2A)  
244 revealed that the element composition and content of the h-BN/LIPG<sub>0</sub> electrode. The  
245 h-BN/LIPG<sub>0</sub> electrode contained C, O, B, N. Zhu [22] has reported the laser direct  
246 writing electrode only contained C and O elements, PI film contained N element, so  
247 the existent of B elements was originated from h-BN.

### 248 3.2 Performance of flexible integrated electrode

249 A LIPG flexible integrated three-electrode consists of an unmodified LIPG  
250 served as counter electrode, drop-coated Ag/AgCl ink on bare LIPG as reference  
251 electrode, h-BN/LIPG<sub>0</sub> as working electrode, and it perfectly plugged into the

252 portable mini-workstation interface, benefiting from its portability, pocket size and  
253 good conductive track. The portable mini-workstation connects wirelessly to a  
254 smartphone via Bluetooth, and the voltammetric analysis was test by the PSTrace  
255 program.

256 To study the electrocatalytic potential of the self-made LIPG flexible integrated  
257 three-electrode to SMZ, four three-electrode systems and two different sensing  
258 devices were established, respectively (Fig. S3). The electrode of LIPG<sub>0</sub> and h-  
259 BN/LIPG<sub>0</sub> (both Ag/AgCl ink was drop-coated as the reference electrode) coupled  
260 with portable mini-workstation. The electrode of LIPG<sub>1</sub> and h-BN/LIPG<sub>1</sub> (both SCE  
261 served as the reference electrode) coupled with traditional workstation were used to  
262 detect the same concentration of SMZ. The result of the electrocatalytic potential  
263 comparison was shown in Fig. 2B. It presented that the electrocatalytic potential of  
264 LIPG<sub>0</sub> (0.59 V) and h-BN/LIPG<sub>0</sub> electrode (0.56 V) on portable mini-workstation both  
265 lower than LIPG<sub>1</sub> (0.76 V) and h-BN/LIPG<sub>1</sub> electrode (0.76 V) on conventional  
266 electrochemical workstation, the peak current of LIPG<sub>0</sub> electrode (4.1  $\mu$ A) and h-  
267 BN/LIPG<sub>0</sub> electrode (8.6  $\mu$ A) was higher than those of LIPG<sub>1</sub> (2.1  $\mu$ A) electrode and  
268 h-BN/LIPG<sub>1</sub> (2.8  $\mu$ A) electrode, respectively. Therefore, with the same working  
269 electrode, the detection effect is better on the portable workstation using flexible  
270 integrated three-electrode than on the traditional non-integrated rigid electrode and  
271 workstation. Surprisingly, the response time of portable mini-workstation using DPV  
272 method was ten times (only about 6 seconds) faster than conventional electrochemical  
273 workstation (at least 60 seconds), this is a valuable feature for on-site rapid detection

274 in comparison [23].

275 The current response and electrocatalytic potential of commercial SPCE to SMZ  
276 of the same concentration on portable mini-workstation were also compared, and the  
277 sensing devices and the results were shown in the Fig. S4A and Fig. S4B,  
278 respectively. The current response of LIPG<sub>0</sub> electrode (4.1  $\mu$ A) and h-BN/LIPG<sub>0</sub> (8.6  
279  $\mu$ A) electrode was larger than that of SPCE (1.3  $\mu$ A) and h-BN/SPCE (3.2  $\mu$ A), the  
280 electrocatalytic potential of LIPG<sub>0</sub> (0.59 V) and h-BN/LIPG<sub>0</sub> (0.56 V) was lower than  
281 SPCE (0.60 V) and h-BN/SPCE (0.66 V). Therefore, the home-made flexible  
282 integrated electrode of h-BN/LIPG<sub>0</sub> had a favorable advantage in lower  
283 electrocatalytic potential, high current response and rapid detection for SMZ.

284 The electrochemical behaviors of ferrous/ferricyanide on h-BN/LIPG<sub>0</sub> and LIPG<sub>0</sub>  
285 electrodes were investigated by CV in 5 mM K<sub>3</sub>[Fe(CN)<sub>6</sub>] and K<sub>4</sub>[Fe(CN)<sub>6</sub>]  
286 containing 0.1 M KCl from the potential range of -0.2 V - 1.2 V at a scan rate of 50  
287 mV s<sup>-1</sup> (Fig. 2C), showing that the potential difference between the oxidation peak  
288 and reduction peak at the h-BN/LIPG<sub>0</sub> electrode was significantly smaller than that of  
289 LIPG<sub>0</sub> electrode. It showed that the electrocatalytic oxidation capacity of the LIPG<sub>0</sub>  
290 electrode modified by h-BN was stronger than that of the LIPG<sub>0</sub> electrode.

291 The cycle stability of the h-BN/LIPG<sub>0</sub> electrode with continuous CVs scans of 50  
292 cycles has unchanged (Fig. 2D). The RSD values of the h-BN/LIPG<sub>0</sub> electrode with  
293 both anode and cathode peak currents were 2.79% and 2.94%, respectively, showing  
294 that the h-BN/LIPG<sub>0</sub> electrode had better electrochemical cycle stability and electrode  
295 stability.

296 Electrochemically effective surface areas ( $A$ ) of the h-BN/LIPG<sub>0</sub> electrode was  
297 determined by chronocoulometry using 5 mM K<sub>3</sub>[Fe(CN)<sub>6</sub>] containing 0.1 M KCl as  
298 supporting electrolyte (Fig. 2E). According to equation (1) of Anson:

$$299 \quad Q(t) = 2nFACD^{1/2}t^{1/2}\pi^{-1/2} + Q_{dl} + Q_{ads} \quad \text{Equation. (1)}$$

300 where  $n$  is the electron number ( $n = 1$ ),  $D$  is the diffusion coefficient involved in  
301 the electrochemical reaction of [Fe(CN)<sub>6</sub>]<sup>3-</sup> solution ( $D = 7.6 \times 10^{-6} \text{ cm}^2 \text{ s}^{-1}$ ),  $C$  is the  
302 substrate concentration, and other symbols have their usual meaning. According to the  
303 linear relationships of  $Q - t^{1/2}$  as shown in Fig. 2F, the effective surface area was  
304 calculated as 0.201 cm<sup>2</sup>, 1.198 cm<sup>2</sup> for the LIPG<sub>0</sub> and h-BN/LIPG<sub>0</sub>, respectively. The  
305 result revealed that the  $A$  of the h-BN/LIPG<sub>0</sub> electrode was 5.96 times greater than the  
306 LIPG<sub>0</sub> electrode and substantially enlarging the electrochemical active sites.

### 307 3.3 Optimization of sensing parameters

308 The modified volume of the h-BN nanoflake solution can affect the  
309 electrochemical signal of the sensor for SMZ. If the modified volume is too little, the  
310 surface of electrode cannot be completely covered and the advantages of modified  
311 materials cannot be fully played. Conversely, the sufficient amounts of modified  
312 materials are more favorable for electron transfer. Therefore, it is necessary to  
313 optimize the amount of electrode modified material. As shown in Fig. 3A, the current  
314 response reached the maximum when the modified volume was 0.6  $\mu\text{L}$ , indicating the  
315 electron transfer performance of the sensor was the best. Therefore, 0.6  $\mu\text{L}$  h-BN  
316 nanoflake solution was modified on LIPG<sub>0</sub> electrode for subsequent experiments.

317 The CVs corresponding to various scan rates ( $v$ ) of 50  $\mu\text{M}$  SMZ on the h-



318 BN/LIPG<sub>0</sub> electrode were investigated in BR of pH 5.0. As shown in Fig. 3B with the  
 319 increase of scan rates from 20 mV s<sup>-1</sup> to 100 mV s<sup>-1</sup>, it was observed that the  
 320 oxidation peak potentials significantly shifted towards a more positive potential. The  
 321 curves of the  $I_{pa}$  increased linearly with the square root of scan rates ( $v^{1/2}$ ,  $R^2 =$   
 322 0.9941, Fig. 3D) and the logarithm of scan rate ( $\ln v$ ,  $R^2 = 0.9941$ , Fig. 3E), but the  
 323 curve showed a bending characteristic with the scan rates ( $v$ , Fig. 3C), revealing that  
 324 the reaction of SMZ could be a typically irreversible diffusion control process. The  
 325 linear relationship between  $E_{pa}$  and  $\ln v$  for SMZ could be expressed as  $E_{pa} = 0.9257 +$   
 326  $0.0665 \ln v$  ( $R^2 = 0.9929$ ) (Fig. 3E), and  $E_{pa}$  could be calculated according to the  
 327 equation (2) of Laviron theory.

$$328 \quad E_{pa} = E^0 + \left(\frac{RT}{\alpha nF}\right) \ln\left(\frac{RTk^0}{\alpha nF}\right) + \left(\frac{RT}{\alpha nF}\right) \ln v \quad \text{Equation. (2)}$$

329 Where  $\alpha$  is the transfer coefficient,  $k^0$  is the rate constant of the reaction,  $v$  is the  
 330 scan rate,  $n$  is the electron-transfer number;  $E^0$  is the formal standard potential,  $R$ ,  $T$ ,  
 331 and  $F$  have their usual meanings ( $R = 8.314 \text{ J mol}^{-1} \text{ K}^{-1}$ ,  $T = 298 \text{ K}$ , and  $F = 96,485 \text{ C}$   
 332  $\text{mol}^{-1}$ ). In general, the value of  $\alpha$  is between 0.3 and 0.7 [34], therefore  $n$  is calculated  
 333 to be 1 from the slope of the linear regression equation, which was in lined with  
 334 previously reported results [35].

335 The electrochemical reaction involves proton-transfer reaction and it is  
 336 influenced by the pH of the electrolyte. The effect of pH on the electrocatalytic  
 337 oxidation of SMZ on h-BN/LIPG<sub>0</sub> was studied by DPV in 0.04 M BR with pH range  
 338 of 3.0 ~ 9.0 (Fig. 3F). There were obvious differences in peak currents ( $I_{pa}$ ) and  
 339 potentials ( $E_{pa}$ ) to SMZ under different pH conditions. The maximum peak current

340 was found at pH value of 5.0. In addition, the linear relationship between  $E_{pa}$  and pH  
341 for SMZ (Fig. 4A) could be expressed as  $E_{pa} = 0.940 - 0.045 \text{ pH}$  ( $R^2 = 0.9947$ ). The  
342 number of proton (m) participating in the electrochemical reaction was calculated  
343 according to Nernst equation (2).

$$344 \quad E_{pa} = E^0 + \left(\frac{RT}{nF}\right)\ln\left(\frac{[\text{Ox}]}{[\text{Red}]}\right) + \left(\frac{2.303mRT}{nF}\right)\text{pH} \quad \text{Equation. (2)}$$

345 Where m is the number of protons in the electrochemical reaction and it could be  
346 further calculated by the slope of the linear regression equation. Thus, m was  
347 calculated to be 1 for SMZ, it was in agreement with the mechanism of the previous  
348 report [36]. The electrocatalytic oxidation mechanism of SMZ on h-BN/LIPG<sub>0</sub> as  
349 shown in Scheme S1.

#### 350 3.4 The fabricated wireless sensor for detecting SMZ

351 The determination of SMZ using DPV at h-BN/LIPG<sub>0</sub> electrode was performed  
352 in BR (pH = 5.0). Scan the blank buffer solution at least 6 times before each test to  
353 stabilize the background current and ensures reproducibility of the electrode in the  
354 voltammetry measurements. The peak current of SMZ increased with its  
355 concentration (Fig. 4B), and there is a linear relationship between anodic peak current  
356 and SMZ concentration in the range from 0.5 to 362.5  $\mu\text{M}$ , its linear equation was  $I_{pa}$   
357  $= 3.5098 C + 0.2154$  ( $R^2 = 0.9963$ , Fig. 4C). The LOD was 0.011  $\mu\text{M}$  (LOD =  $3 \sigma/m$ ,  
358 where  $\sigma$  is the standard deviation of 20 times electrochemical responses for the blank  
359 solution and m is the slope of the calibration plot) and the LOQ was 0.037  $\mu\text{M}$ . In  
360 comparison with previous reported results (Table S1), it could be observed that the  
361 fabricated h-BN/LIPG<sub>0</sub> sensor was not only easy to use, but had a low electrochemical

362 oxidation potential, a low LOD, and widespread linear ranges for SMZ. These results  
363 indicated that the h-BN/LIPG<sub>0</sub> electrode was an excellent electrochemical sensing  
364 electrode for the detection of SMZ.

### 365 3.5 Repeatability, reproducibility and selectivity

366 The repeatability of the h-BN/LIPG<sub>0</sub> electrode for the voltammetric response of  
367 50  $\mu$ M SMZ was estimated using the same modified by 20th successive  
368 measurements under the optimum conditions. As shown in Fig. 4D, the RSD value of  
369 the repeatable peak currents was 4.01%, showing a good repeatability of the proposed  
370 sensor. The reproducibility of the prepared ten h-BN/LIPG<sub>0</sub> electrodes was evaluated  
371 for the determination of SMZ under the same conditions, respectively, the RSD value  
372 was 4.65% (Fig. 4E), indicating that the sensor had good reproducibility. In order to  
373 investigate the effect of bending on the performance of the h-BN/LIPG<sub>0</sub> electrode, the  
374 current response before and after bending 50 times were studied, and the result  
375 showed that the current was almost the same before and after bending.

376 The selectivity for the voltammetric detection of SMZ at the h-BN/LIPG<sub>0</sub>  
377 electrode was investigated and indicated in Fig. 4F. Firstly, 50  $\mu$ M SMZ was added  
378 and detected in 0.04 M BR (pH = 5.0), then, the possible interferents such as NaCl,  
379 KCl, MgCl<sub>2</sub>, CaCl<sub>2</sub> with 100-fold concentration, glucose with 10-fold concentration  
380 of SMZ were added successively and tested in the presence of 50  $\mu$ M SMZ. Glutamic  
381 acid, arginine and hypoxanthine with 1-fold concentration of SMZ were also tested.  
382 The results in Fig. 4F indicated that the determination of SMZ not influenced (RSD  
383 value < 5%) by the possible interfering substances, hence, the obtained sensors had a

384 good anti-interferent ability for SMZ.

385 In the previous voltammetry sensors, many studies only focused on the detection  
386 of single sulfonamide, but few studies analyzed the effect of sulfonamide analogs to  
387 the current response of SMZ [36-40]. In this work, we tested the influence of current  
388 repose in the presence of the equal amount of SN and SM2, the change value of SMZ  
389 current response was 10.3% and 10.9%, respectively. It is possible that the  
390 sulfonamide analogues have very similar oxidation potentials, so the simultaneous  
391 detection of multi-sulfa antibiotics by voltammetric methods still presents high mutual  
392 interference [41].

### 393 3.6 Practical application of portable sensor

394 The feasibility and applicability of the proposed h-BN/LIPG<sub>0</sub> sensor for the  
395 detection of SMZ were performed by the portable sensor based on a smartphone and a  
396 reference HPLC method (national standard method of China) in lake water and milk  
397 (Table 1). The RSD values were less than 5% and recoveries of the samples were in  
398 the range of 97.5 – 108.2% of the two methods, indicating that the proposed method  
399 had a satisfactory precision and feasibility. Moreover, the results of the proposed  
400 portable sensor and the HPLC method were compared by the paired t-test with SPSS  
401 (22.0) Statistical Analysis Software (Table S2). Results of analysis showed there was  
402 no significant difference between the two methods, which also suggesting a promising  
403 practical application in spiked sample analyses of the portable sensor.

404 The proposed method was used to detection other four SAs (SN, SIZ, SM2,  
405 SPY) with linear concentration range of 2.08  $\mu\text{M}$  to 233.33  $\mu\text{M}$ . The voltammogram

406 and corresponding linear relationships were demonstrated in Fig. 5. It indicated that  
407 the electrochemical oxidation potential of four SAs were similar with SMZ and there  
408 was a good linear relationship between concentrations and current responses on the h-  
409 BN/LIPG<sub>0</sub> electrode, the R<sup>2</sup> values were 0.9887, 0.9871, 0.9955 and 0.9868,  
410 respectively. This may be due to the fact that all five SAs have the structure of  
411 benzenesulfonamide, so the catalytic potential is very close, which was consistent  
412 with the previous interference experiment. However, in the rational use of drugs,  
413 generally only one sulfonamide is used to prevent or treat mild infection. So, through  
414 the linear equations of five SAs, it can be seen that the proposed portable, fast sensing  
415 method had a good effect in detecting these five SAs, respectively.

#### 416 **4. Conclusion**

417 A home-made flexible integrated three-electrode fabricated by laser writing  
418 technology as a low-cost, portable and fast sensing platform was successfully  
419 developed for electrochemical detection of SAs. The novel flexible integrated three-  
420 electrode has the characteristics of easy-to-prepare, low cost, 3D porous  
421 interconnected network, larger effective surface area, high stability, good selectivity,  
422 low oxidation potential and satisfactory recoveries to SMZ. It has been confirmed that  
423 the proposed method has no difference with HPLC method and can be used for the  
424 detection of five SAs. Such miniaturized integrated electrode could allow testing for  
425 SAs to more reliable, easier and inexpensive, and has enormous potential in outdoor  
426 analysis.

427

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432 **References**

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596 **Figure caption :**

597 **Fig. 1.** SEM (A, B), cross-sectional SEM (C, D), and TEM (E, F) of LIPG<sub>0</sub>. SEM (G,  
598 H), cross-sectional SEM (I, J) and TEM (K, L) of h-BN/LIPG<sub>0</sub>. HAADF-STEM  
599 image (inserted in M) of h-BN/LIPG<sub>0</sub> electrode and corresponding EDX-mapping  
600 images mapping images of C element (M), O element (N), B element (O) and N  
601 element (P).

602 **Fig. 2.** (A) EDS elemental analyses of h-BN/LIPG<sub>0</sub>; (B) Comparison of peak  
603 potentials to SMZ detected by h-BN modified LIPG electrodes using different  
604 reference electrodes (Ag/AgCl ink or SCE); (C) Cyclic voltammetric behavior (scan  
605 rate was 100 mV s<sup>-1</sup>) of SMZ at LIPG<sub>0</sub> and h-BN/LIPG<sub>0</sub> electrodes in the same  
606 concentration of SMZ; (D) Stability of with successive CVs scans of 50 cycles of h-  
607 BN/LIPG<sub>0</sub> electrode; (E) The plots of  $Q - t$  curves of SMZ at LIPG<sub>0</sub> and h-BN/LIPG<sub>0</sub>  
608 electrodes; (F) The plots of  $Q - t^{1/2}$  curves of SMZ at LIPG<sub>0</sub> and h-BN/LIPG<sub>0</sub>  
609 electrodes.

610 **Fig. 3.** (A) Optimization of modification amount of h-BN at h-BN/LIPG<sub>0</sub> electrode;

611 (B) CV curves of h-BN/LIPG<sub>0</sub> from 20 - 100 mV s<sup>-1</sup>; Plots of  $v - I$  (C),  $v^{1/2} - I$  (D),  $\ln v$   
612  $- E$  (E) were presented; (F) DPV of  $5 \times 10^{-5}$  mol/L SMZ with different pH values at h-  
613 BN/LIPG<sub>0</sub> electrode.

614 **Fig. 4.** (A) The effect of different pH on oxidation peak potentials (straight line) and  
615 oxidation peak current values (curve) for SMZ in 0.04 M BR with scan rate 100 mV s<sup>-1</sup>;  
616 (B) DPV of SMZ at h-BN/LIPG<sub>0</sub> electrode in 0.04 M BR containing concentration  
617 from 0.5 - 362.5  $\mu$ M at h-BN/LIPG<sub>0</sub> electrode; (C) The linear equation of SMZ with  
618 different concentration from 0.5 - 36.25  $\mu$ M; repeatability (D) and reproducibility (E)  
619 of h-BN/LIPG<sub>0</sub> electrode for the determination of  $5 \times 10^{-5}$  mol/L SMZ in BR (pH  
620 5.0); (F) Adding SMZ (a), NaCl (b), KCl (c), MgCl<sub>2</sub> (d), CaCl<sub>2</sub> (e), glucose (f),  
621 glutamic acid (g), arginine (h) and hypoxanthine (i) in order in the same buffer to  
622 study the effect of possible interfering substances on SMZ detection.

623 **Fig. 5** The proposed wireless and flexible electrochemical sensor based on  
624 smartphone for the detection of four SAs with linear concentration range of 2.08  $\mu$ M  
625 to 233.33  $\mu$ M and corresponding linear relationships: SN (A, B), SIZ (C, D), SM2 (E,  
626 F), SPY (G, H).

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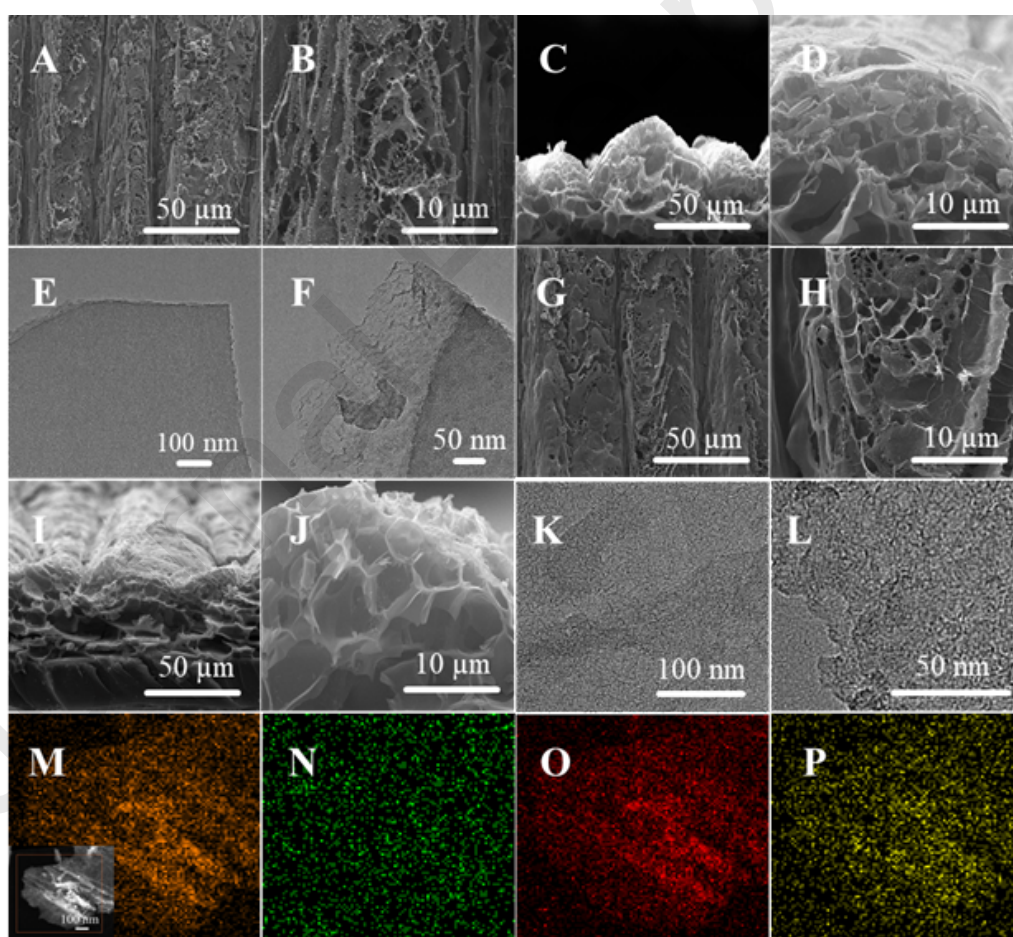
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648 **Fig. 1.** SEM (A, B), cross-sectional SEM (C, D), and TEM (E, F) of LIPG<sub>0</sub>. SEM (G,649 H), cross-sectional SEM (I, J) and TEM (K, L) of h-BN/LIPG<sub>0</sub>. HAADF-STEM



650 image (inserted in M) of h-BN/LIPG<sub>0</sub> electrode and corresponding EDX-mapping  
 651 images mapping images of C element (M), O element (N), B element (O) and N  
 652 element (P).

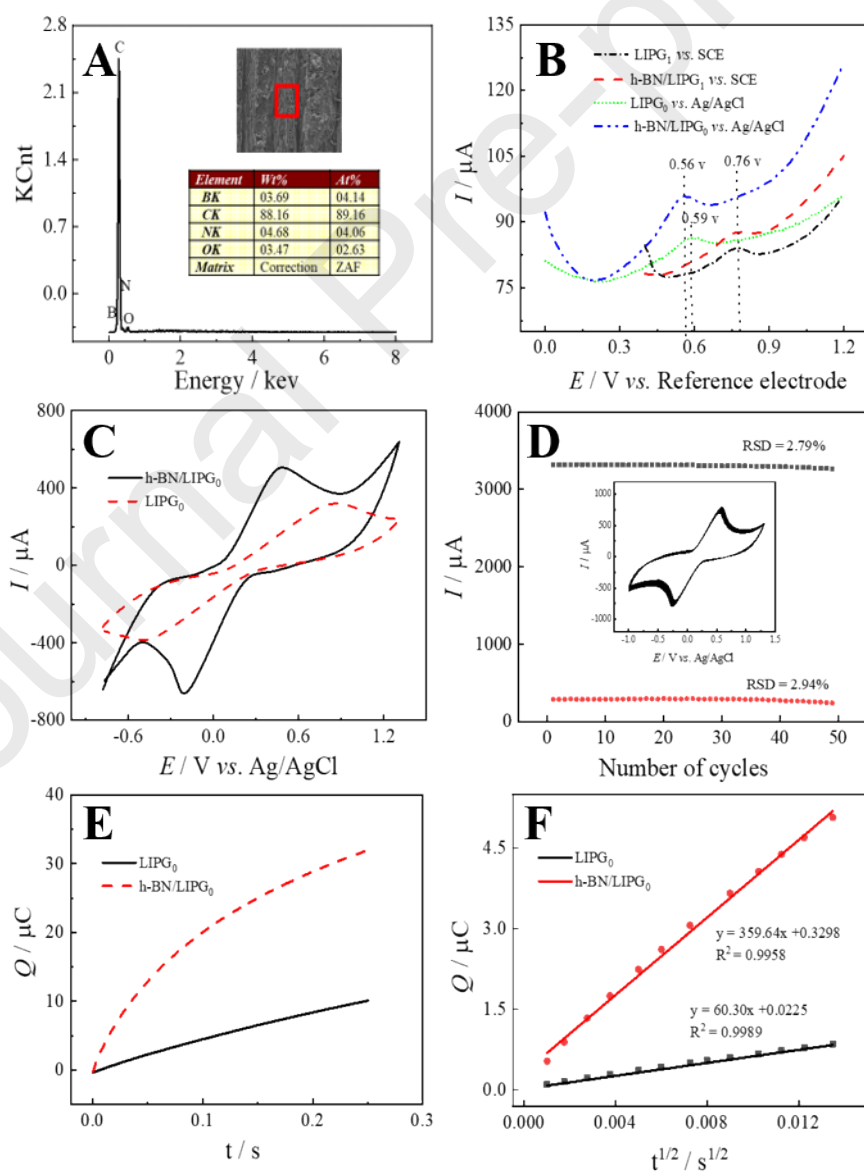
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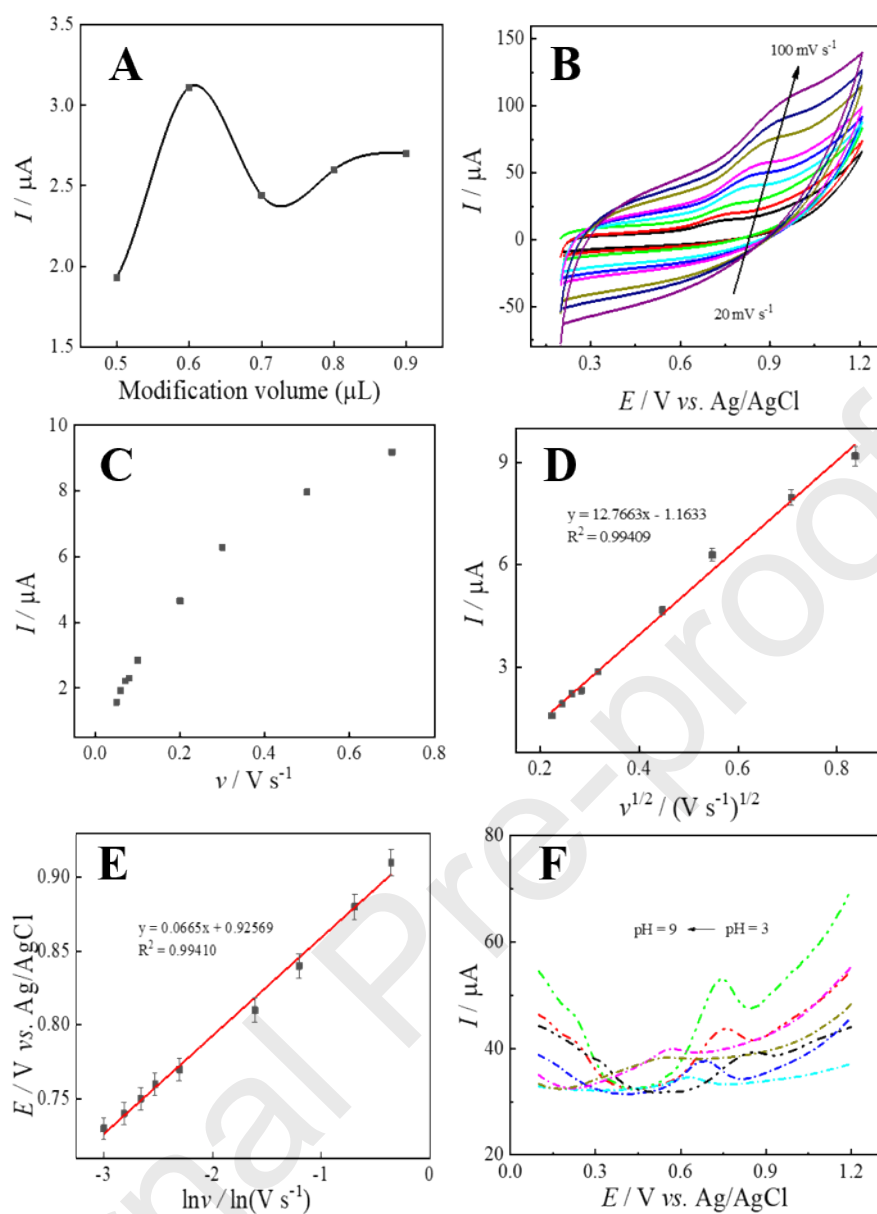
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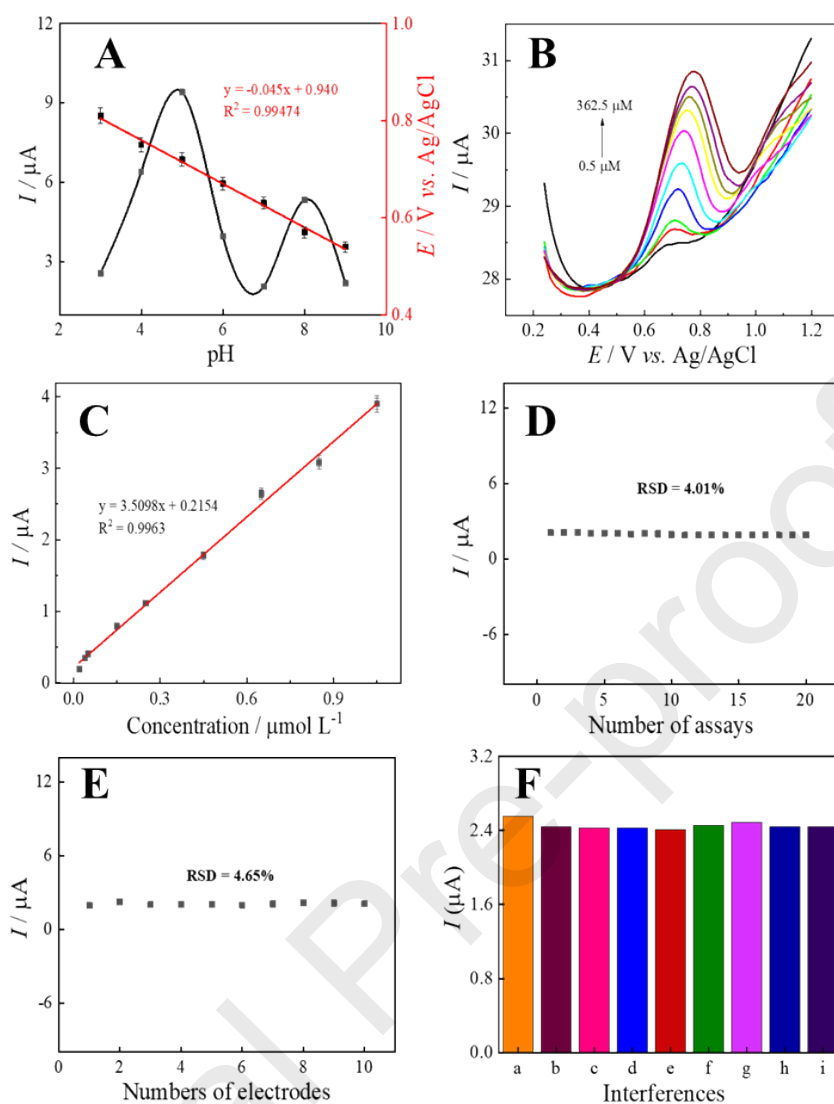
659 **Fig. 2.** (A) EDS elemental analyses of h-BN/LIPG<sub>0</sub>; (B) Comparison of peak  
660 potentials to SMZ detected by h-BN modified LIPG electrodes using different  
661 reference electrodes (Ag/AgCl ink or SCE); (C) Cyclic voltammetric behavior (scan  
662 rate was 100 mV s<sup>-1</sup>) of SMZ at LIPG<sub>0</sub> and h-BN/LIPG<sub>0</sub> electrodes in the same  
663 concentration of SMZ; (D) Stability of with successive CVs scans of 50 cycles of h-  
664 BN/LIPG<sub>0</sub> electrode; (E) The plots of  $Q - t$  curves of SMZ at LIPG<sub>0</sub> and h-BN/LIPG<sub>0</sub>  
665 electrodes; (F) The plots of  $Q - t^{1/2}$  curves of SMZ at LIPG<sub>0</sub> and h-BN/LIPG<sub>0</sub>  
666 electrodes.



667

668 **Fig. 3.** (A) Optimization of modification amount of h-BN at h-BN/LIPG<sub>0</sub> electrode;669 (B) CV curves of h-BN/LIPG<sub>0</sub> from 20 - 100 mV s<sup>-1</sup>; Plots of  $v - I$  (C),  $v^{1/2} - I$  (D),  $\ln v$ 670  $- E$  (E) were presented; (F) DPV of  $5 \times 10^{-5}$  mol/L SMZ with different pH values at h-671 BN/LIPG<sub>0</sub> electrode.

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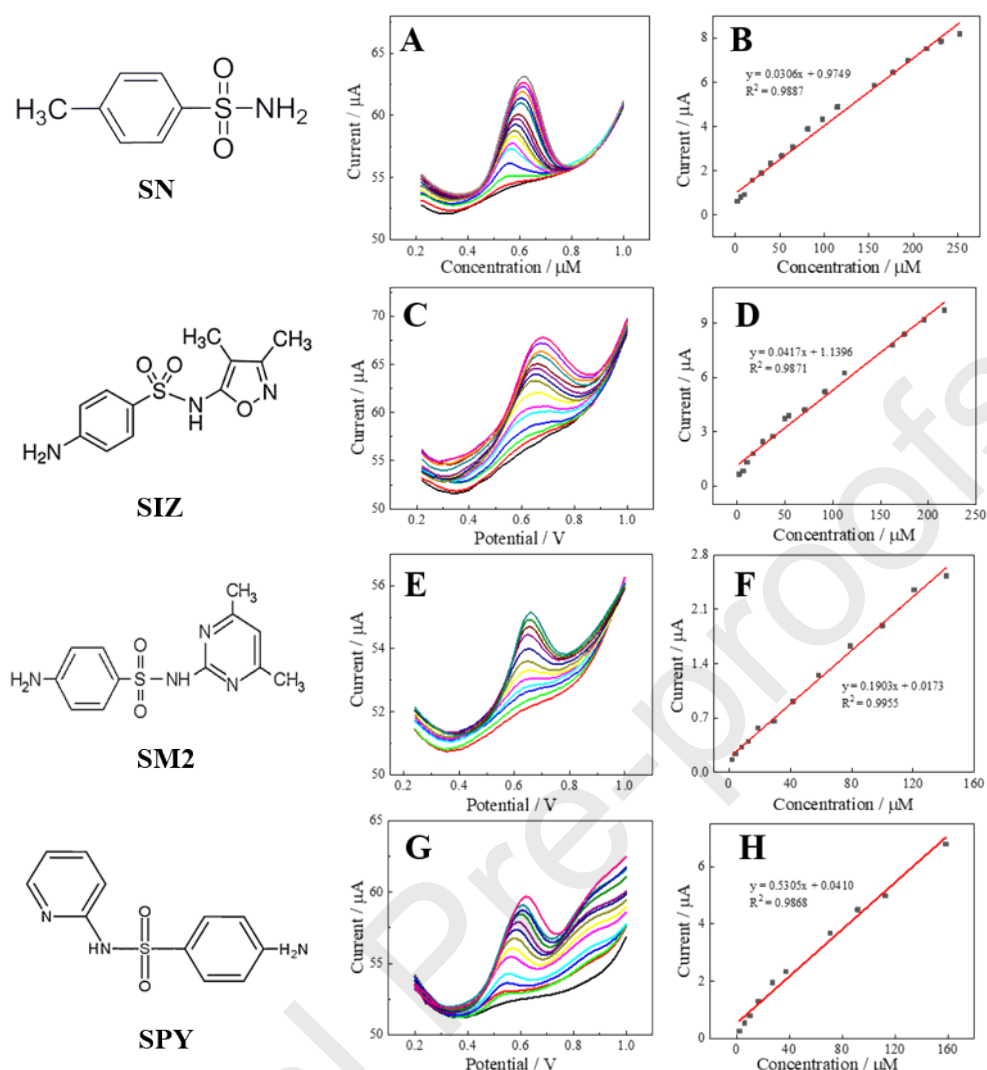


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674 **Fig. 4.** (A) The effect of different pH on oxidation peak potentials (straight line) and675 oxidation peak current values (curve) for SMZ in 0.04 M BR with scan rate 100 mV s<sup>-1</sup>;676 (B) DPV of SMZ at h-BN/LIPG<sub>0</sub> electrode in 0.04 M BR containing concentration677 from 0.5 - 362.5  $\mu\text{M}$  at h-BN/LIPG<sub>0</sub> electrode; (C) The linear equation of SMZ with678 different concentration from 0.5 - 36.25  $\mu\text{M}$ ; repeatability (D) and reproducibility (E)679 of h-BN/LIPG<sub>0</sub> electrode for the determination of  $5 \times 10^{-5}$  mol/L SMZ in BR (pH680 5.0); (F) Adding SMZ (a), NaCl (b), KCl (c), MgCl<sub>2</sub> (d), CaCl<sub>2</sub> (e), glucose (f),

681 glutamic acid (g), arginine (h) and hypoxanthine (i) in order in the same buffer to

682 study the effect of possible interfering substances on SMZ detection.



683

684 **Fig. 5** The proposed wireless and flexible electrochemical sensor based on  
 685 smartphone for the detection of four SAs with linear concentration range of 2.08  $\mu\text{M}$   
 686 to 233.33  $\mu\text{M}$  and corresponding linear relationships: SN (A, B), SIZ (C, D), SM2 (E,  
 687 F), SPY (G, H).

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690 **Table 1.** Recoveries obtained from real samples with the added SMZ using portable  
 691 sensor and HPLC method.

Name	Spiked	Portable sensor	HPLC method
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	( $\mu\text{M}$ )	Found <sup>a</sup> ( $\mu\text{M}$ )	RSD (%)	Recovery (%)	Found <sup>a</sup> ( $\mu\text{M}$ )	RSD (%)	Recovery (%)
	0.00	N. D	-	-	N. D	-	-
Milk	27.50	27.01 $\pm$ 0.036	1.96	98.2	29.56 $\pm$ 0.031	1.97	107.5
	55.00	55.71 $\pm$ 0.017	2.11	101.3	59.51 $\pm$ 0.056	1.05	108.2
	0.00	N. D	-	-	N. D	-	-
Lake water	27.50	26.81 $\pm$ 0.023	2.91	97.5	28.32 $\pm$ 0.004	2.13	103.0
	55.00	54.39 $\pm$ 0.085	3.08	98.9	54.56 $\pm$ 0.012	2.01	99.2

692 <sup>a</sup> Average value of three determinations  $\pm$  relative deviation, N.D: Not detected.

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### 694 **Author statement**

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696 Manuscript title: MICROC-D-22-01014

697 I have made substantial contributions to the conception or design of the work; or the acquisition,

698 analysis, or interpretation of data for the work; AND

699 I have drafted the work or revised it critically for important intellectual content; AND I have

700 approved the final version to be published; AND

701 I agree to be accountable for all aspects of the work in ensuring that questions related to the

702 accuracy or integrity of any part of the work are appropriately investigated and resolved.

703 All persons who have made substantial contributions to the work reported in the manuscript,

704 including those who provided editing and writing assistance but who are not authors, are named in

705 the Acknowledgments section of the manuscript and have given their written permission to be

706 named. If the manuscript does not include Acknowledgments, it is because the authors have not

707 received substantial contributions from nonauthors.

708 Attachment: Yes  No

709 Yifang Zeng

710 August 11, 2022

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713 **Declaration of interests**

714

715  The authors declare that they have no known competing financial interests or personal  
716 relationships that could have appeared to influence the work reported in this paper.

717

718  The authors declare the following financial interests/personal relationships which may be  
719 considered as potential competing interests:

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728 **Scheme 1.** Schematic illustration of the prepared of home-made integrated h-

729 BN/LIPG<sub>0</sub> electrode and as a smartphone-based wireless platform for portable and

730 fast detection of sulfonamides.

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732

733 **Highlights**

734 ● A laser-induced porous graphene as integrated flexible three-electrode was  
735 developed;

736 ● A hexagonal boron nitride modified porous graphene as working electrode was  
737 developed;

738 ● Smartphone-based wireless and flexible electrochemical sensor for sulfonamides  
739 was developed;

740 ● A portable method for outdoor sensing was developed using the home-made  
741 integrated flexible three-electrode.

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